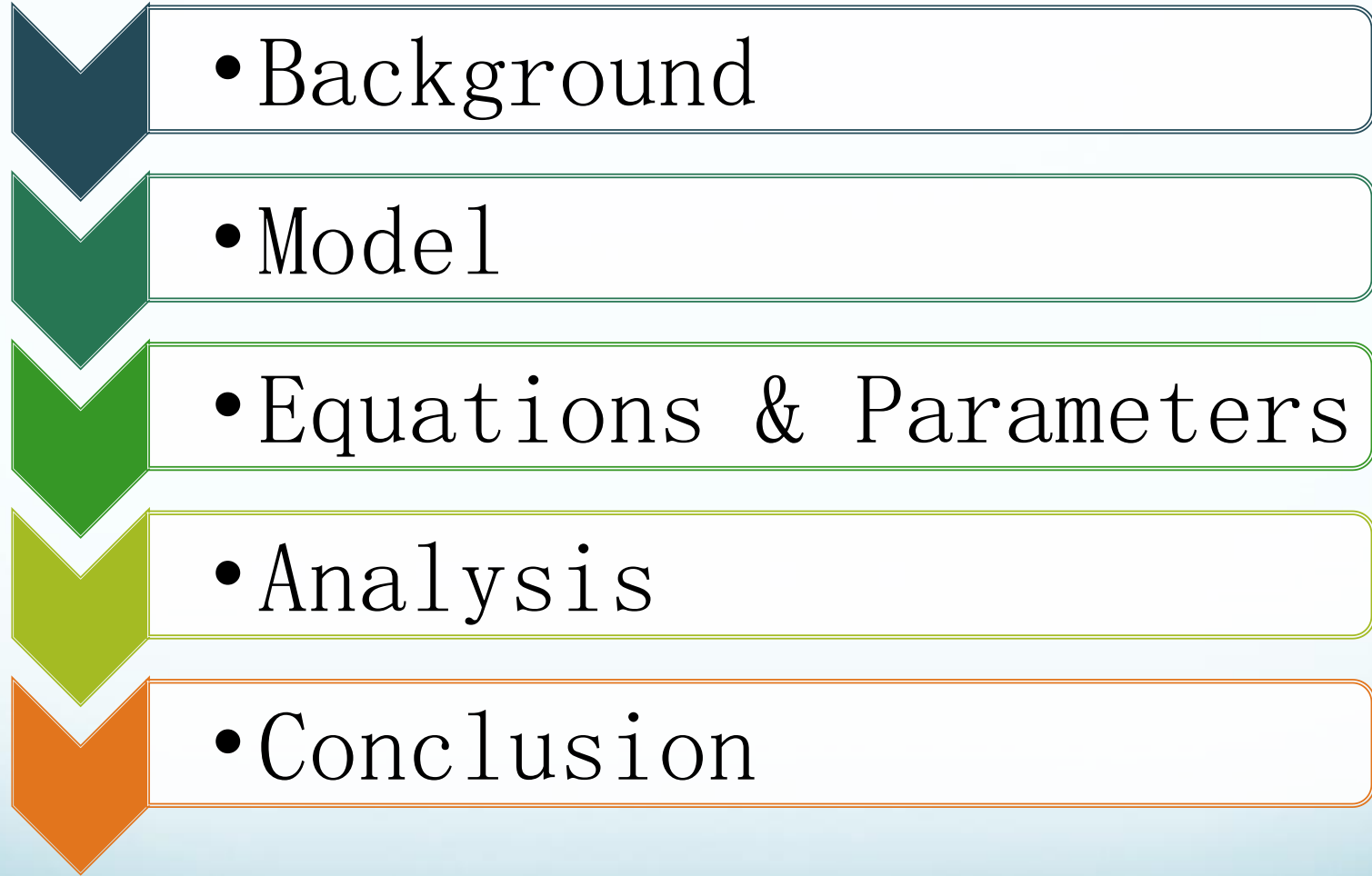


Shock-induced termination of cardiac arrhythmias

Baltazar Chavez-Diaz; Sarah Schwenck; Weide Wang;
Jinglei Zhang; Chen Jiang
Mentor: Williams Katie

Presentation Overview



Background

Model

Equations &
Parameters

Analysis

Conclusion

Cardiac Arrhythmias

Cardiac dysrhythmia or irregular heartbeat

Irregular Electrical activity of the heart

Regular or irregular

Background

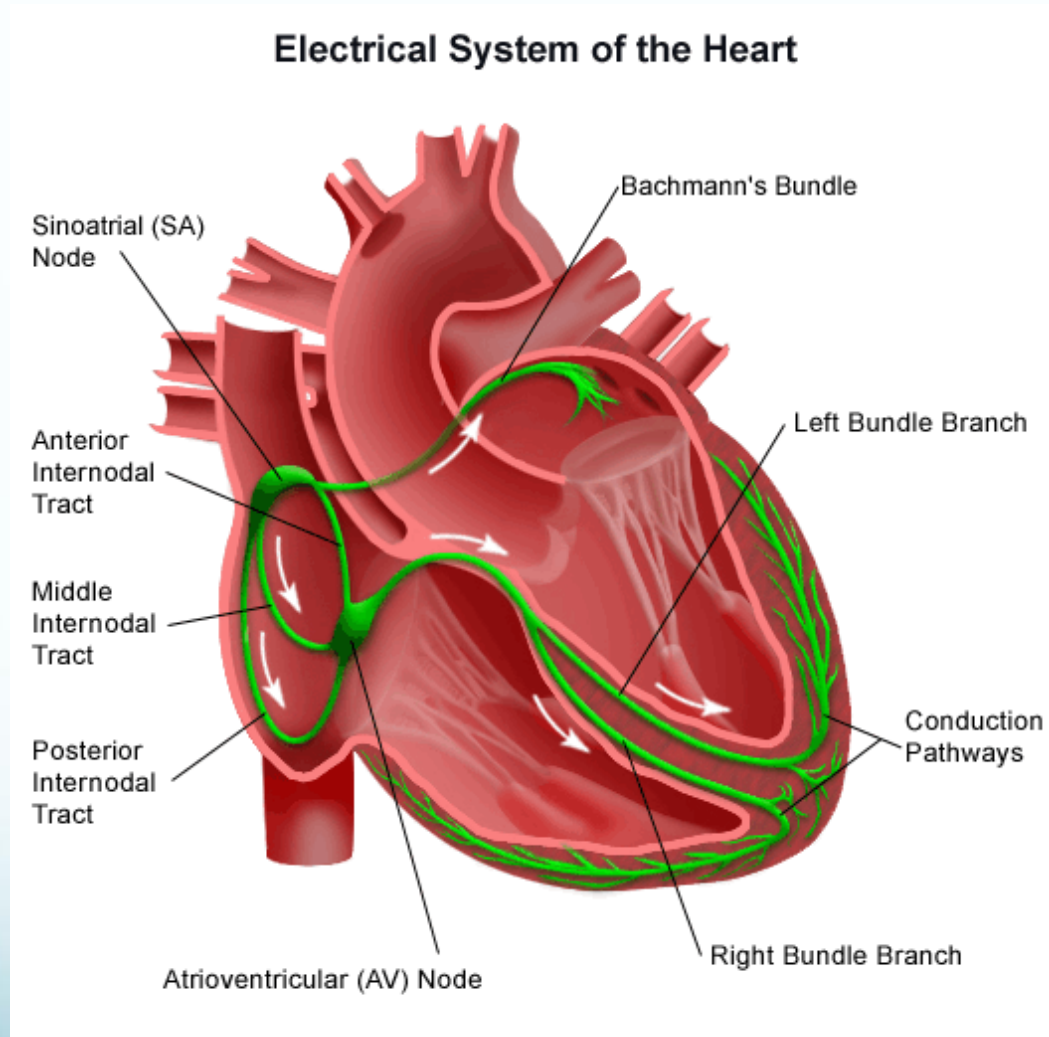
Model

Equations &
Parameters

Analysis

Conclusion

Cardiac Arrhythmias



Background

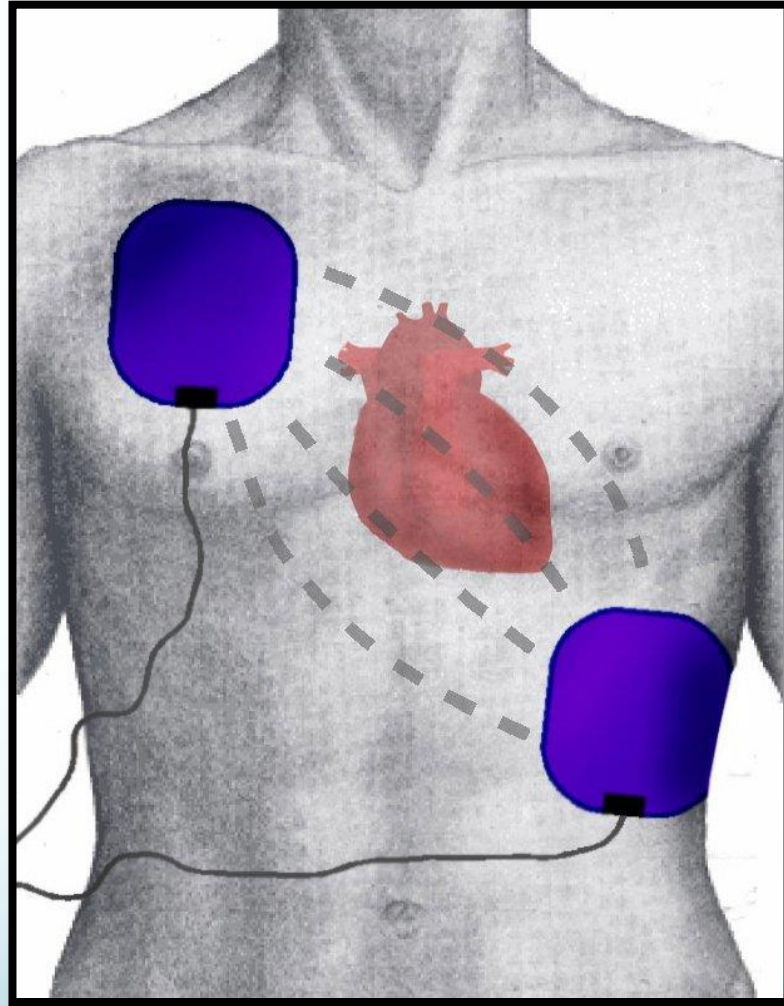
Model

Equations &
Parameters

Analysis

Conclusion

Defibrillators



Background

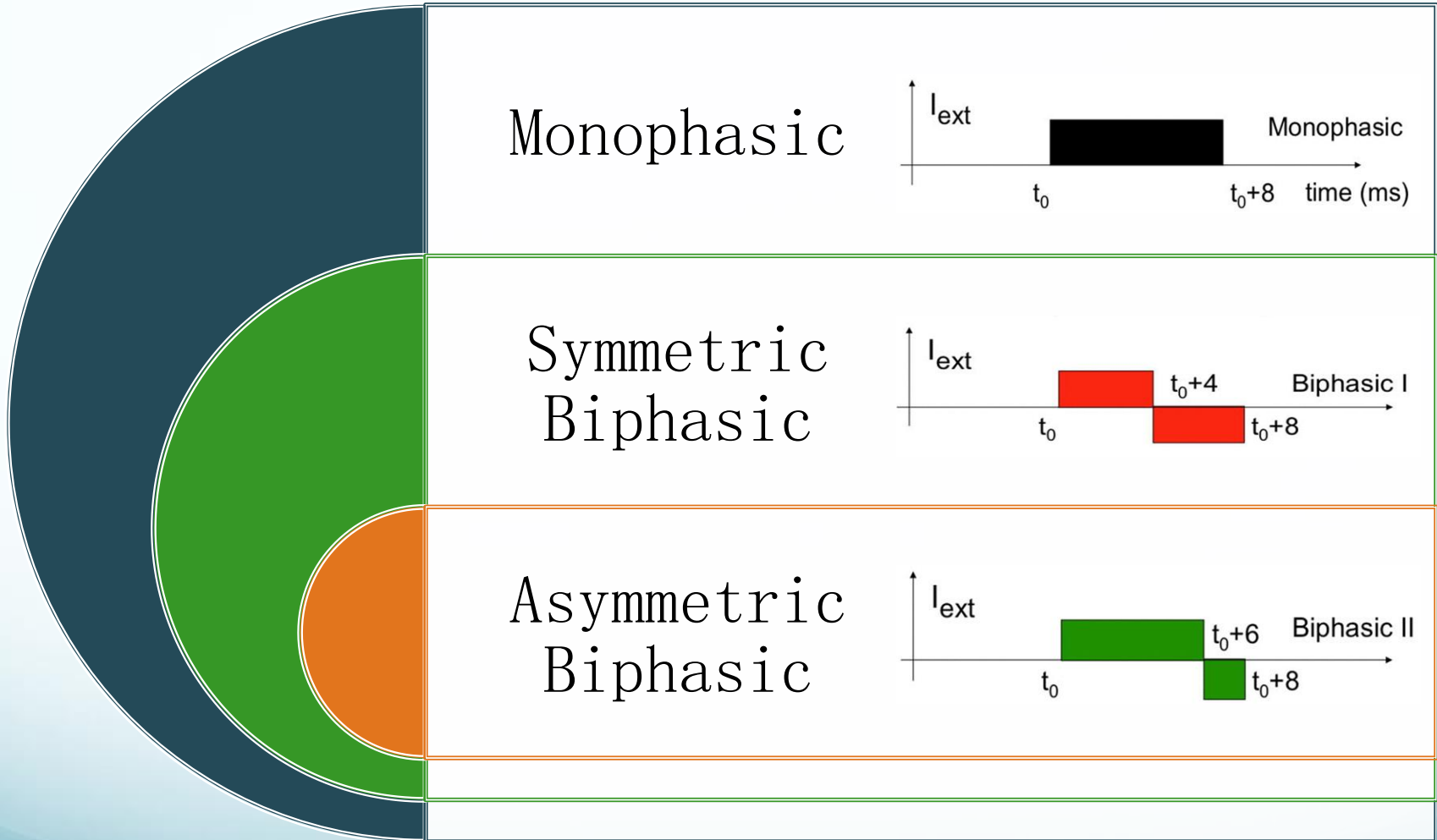
Model

Equations &
Parameters

Analysis

Conclusion

Defibrillators



Background

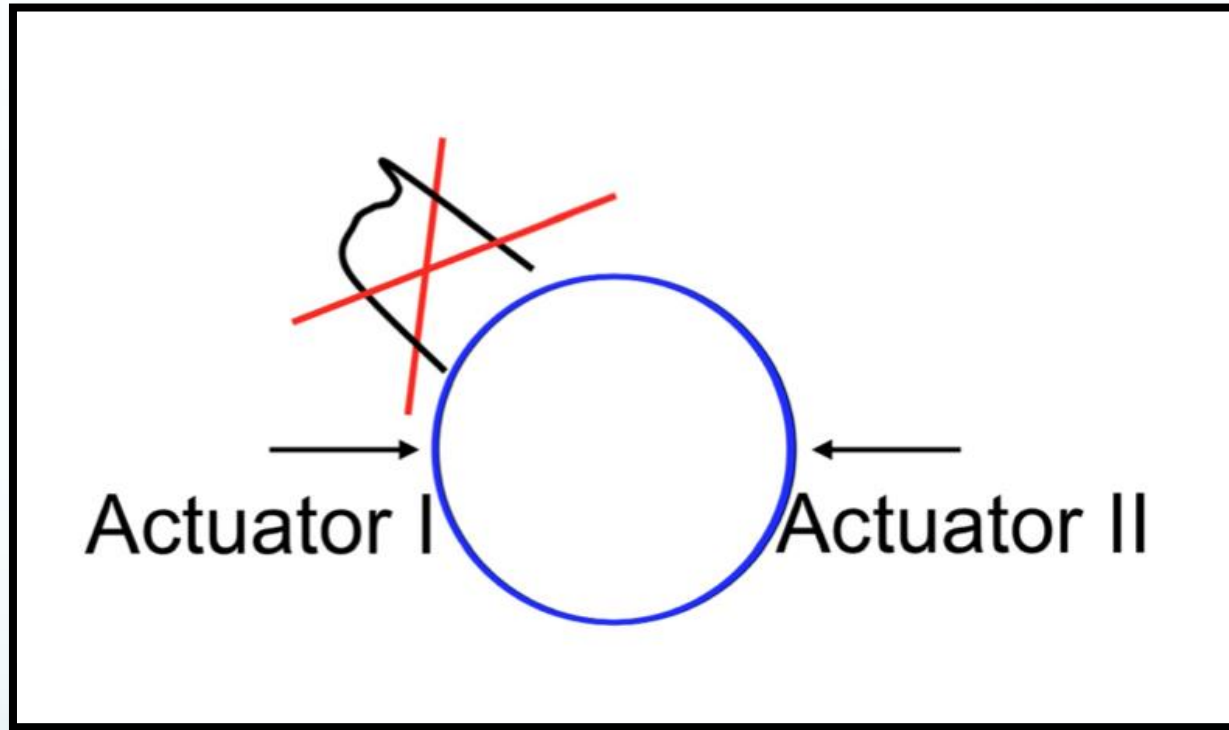
Model

Equations &
Parameters

Analysis

Conclusion

Model



Background

Model

Equations &
Parameters

Analysis

Conclusion

Beeler–Reuter Equation

Describe the electrical activity of cardiac myocytes

Background

Model

Equations &
Parameters

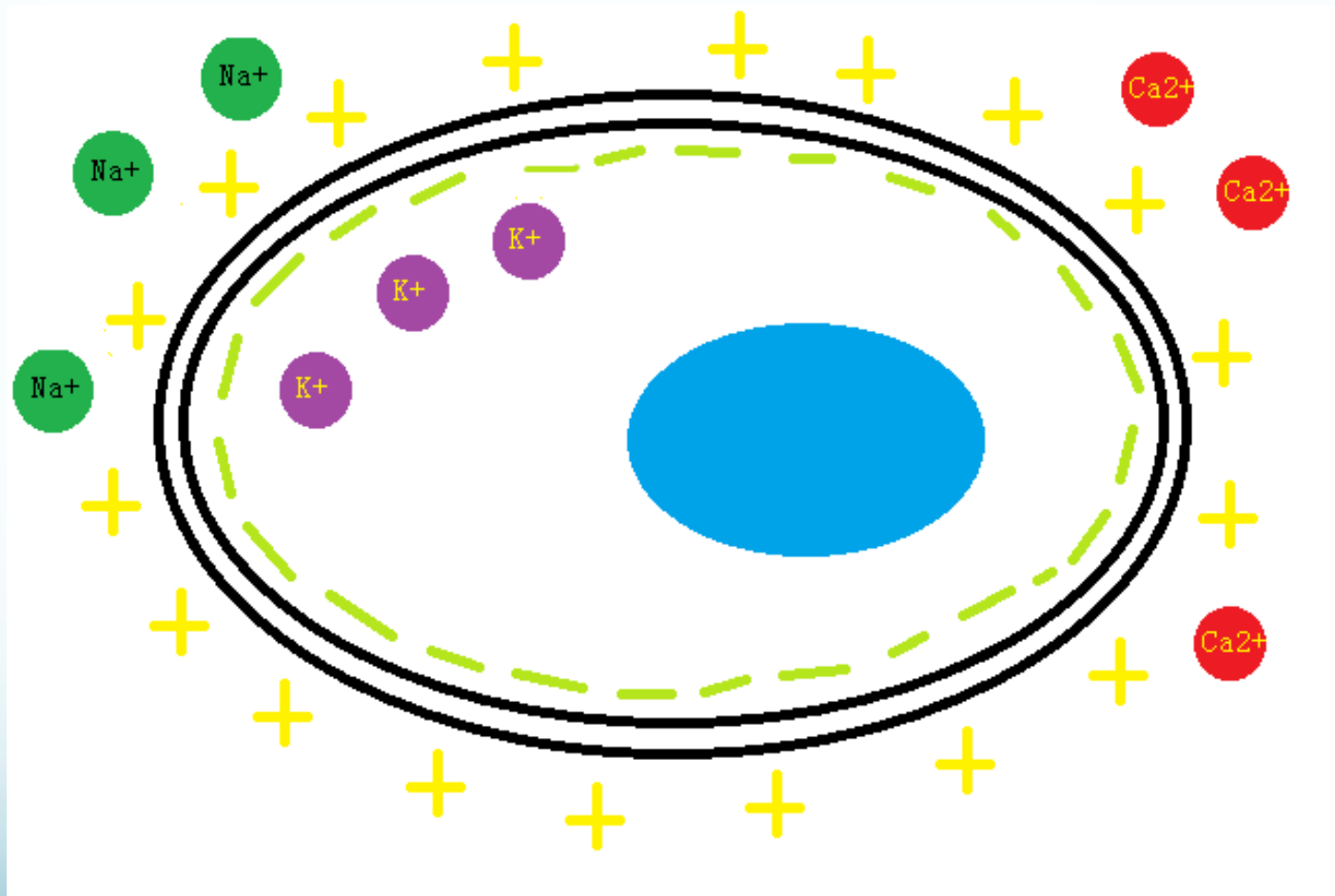
Analysis

Conclusion

Beeler–Reuter Equation

- $$\frac{\partial V_m}{\partial t} = -\frac{I_{BR} + I_{ep} + I_{fu}}{C_m} + \nabla \cdot (D_g \cdot \nabla V_m) + \nabla \cdot (D_g \cdot \nabla \varphi_e)$$
- V_m : membrane potential
- φ_e : extra-cellular potential
- D_g : intra-cellular diffusion of the electrical potential
- C_m : Capacitance per surface area of the myocyte membrane
- $I_{BR} = I_k + I_x + I_{Na} + I_s$

$$I_{BR} = I_K + I_x + I_{Na} + I_s$$



- $$\frac{\partial V_m}{\partial t} = -\frac{I_{BR} + I_{ep} + I_{fu}}{C_m} + \nabla \cdot (D_g \cdot \nabla V_m) + \nabla \cdot (D_g \cdot \nabla \varphi_e)$$

Electroporation phenomenon

$$I_{ep}$$

- When the strength of the applied electric field exceeds a few V/cm, reversible pores are created in the myocyte membrane that allow for ion flow across the membrane.
- As a result, the membrane potential V_m saturates and does not reach unphysiological values for either depolarization or hyperpolarization.

- I_{fu} is an additional current that is needed to account for the possible anode break stimulation of the tissue.

Numerical techniques

$$L = 6.7 \text{ cm}$$

$$dx = 0.025 \text{ cm}$$

- Spatial discretization

$$dt = 0.001 \text{ ms}$$

- During the shock and for the subsequent 10ms and then the time step is changed back to $dt = 0.01 \text{ ms}$ for the rest of the simulation.

Parameter influencing the defibrillation outcome

- 1) The shock waveform
- 2) The shock duration
- 3) The shock energy
- 4) Shock timing
- 5) Dynamical state at the time of the shock
- 6) Heterogeneity of the cardiac tissue
- 7) System size

Background

Model

Equations &
Parameters

Analysis

Conclusion

Simulations

Classification using Artificial Neural Networks (ANN)

- Direct Block, Annihilation, Delayed Block, and Direct Activation

Dose response curves

Analysis of shock timing and size of the action potential

Background

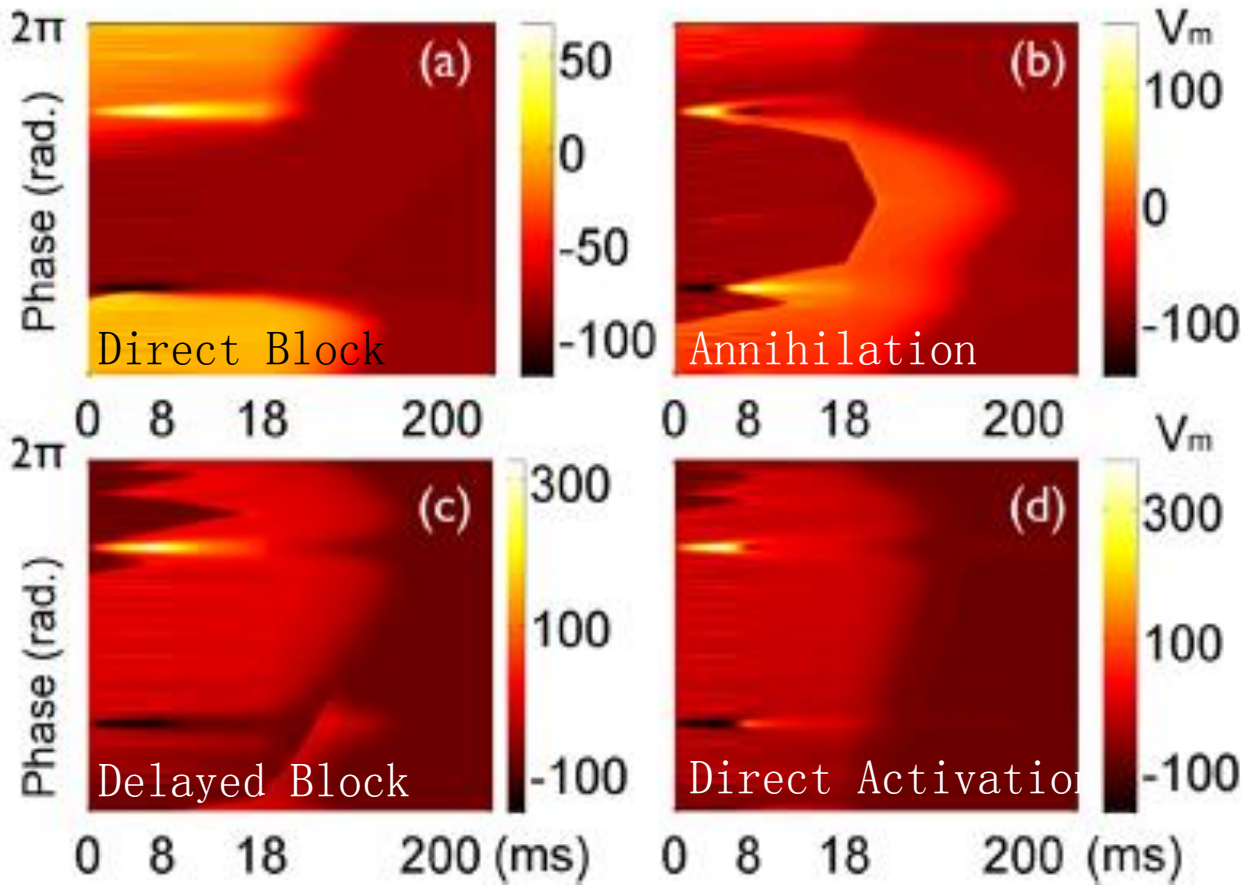
Model

Equations &
Parameters

Analysis

Conclusion

Mechanism Classification



Compute the location and direction of waveforms present

Use this as input for ANN

Background

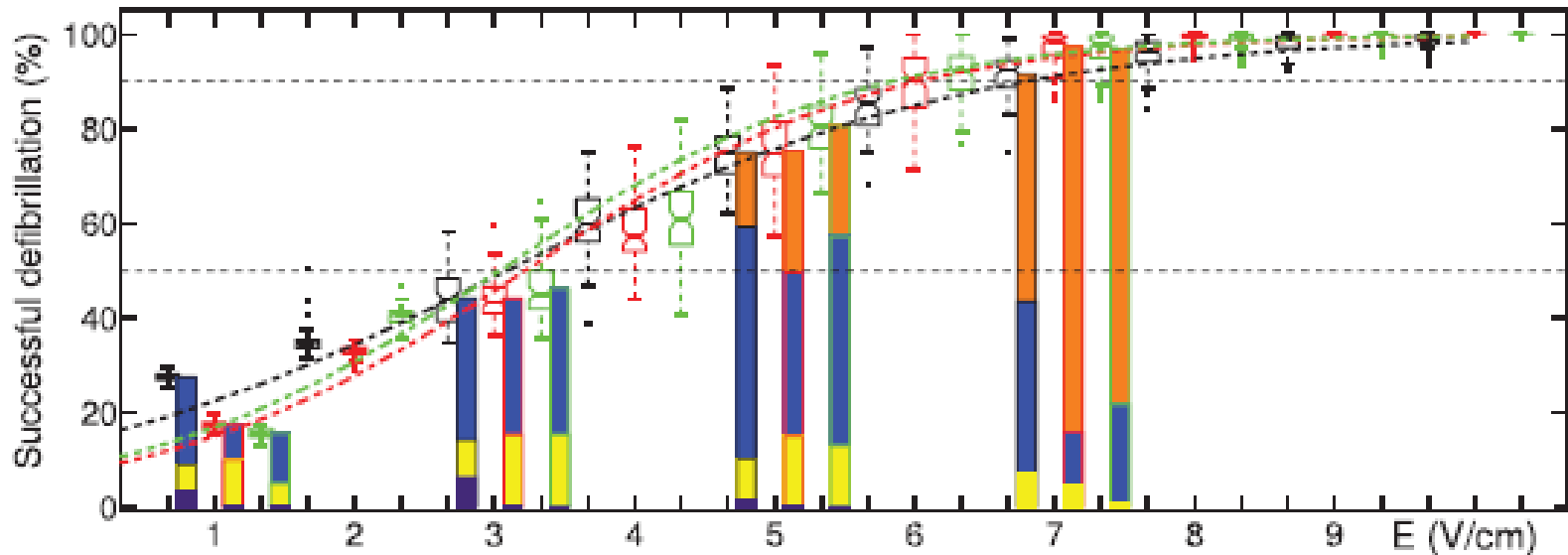
Model

Equations & Parameters

Analysis

Conclusion

Mechanism abundance changes with shock energy



Direct Block mechanism only present in monophasic

Direct Activation mechanism more prominent at higher energies

Background

Model

Equations &
Parameters

Analysis

Conclusion

Dose Response Curves

- $\log\left(\frac{p}{1-p}\right) = \beta_0 + \beta_1 E$
- p is probability of successful defibrillation

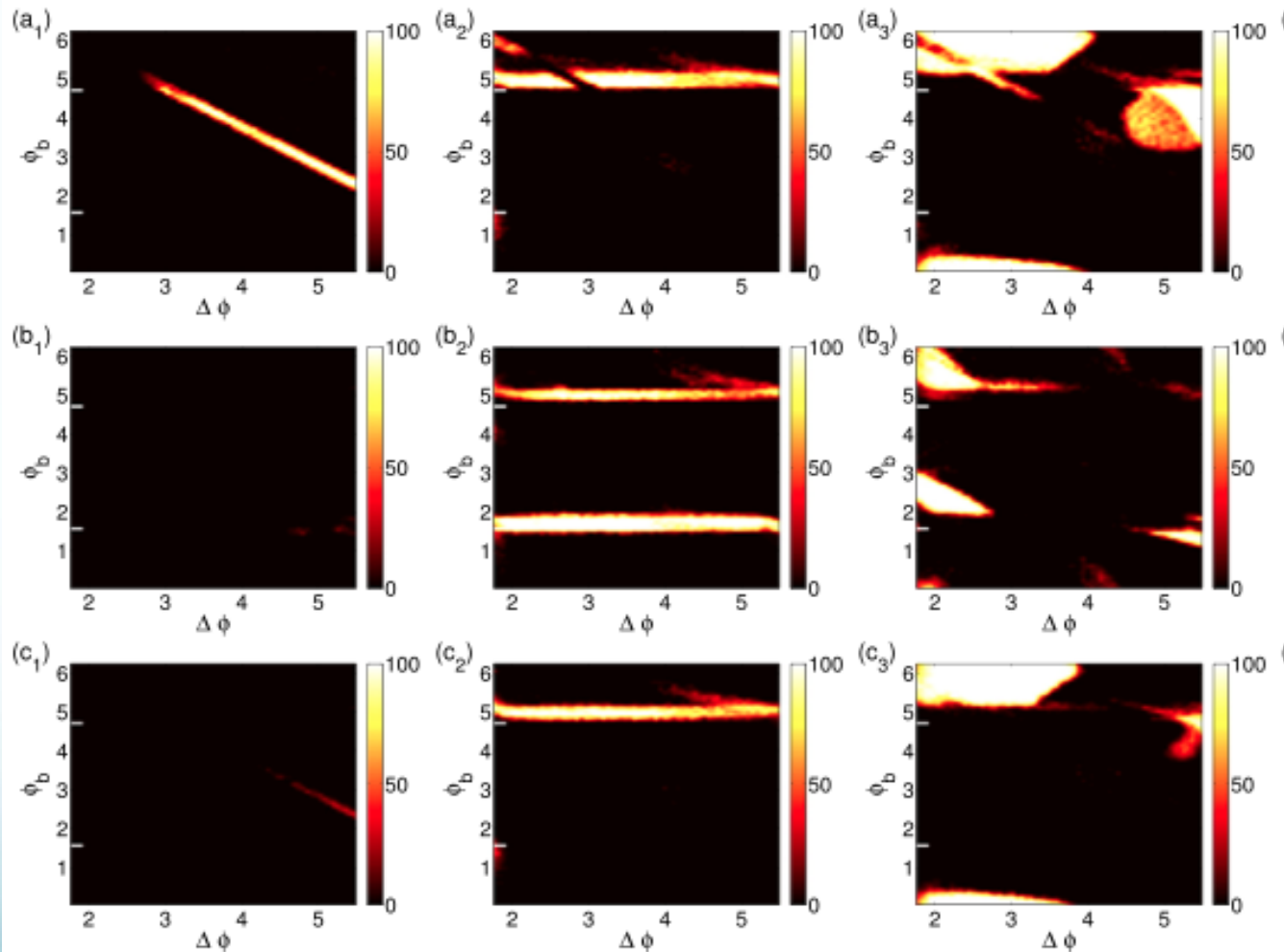
Protocols	Fit parameters	E_{50} (V/cm)	E_{90} (V/cm)
Monophasic	$\beta_0 = -1.835_{(.004)}$ $\beta_1 = 0.5942_{(.001)}$	[3.08 – 3.10]	[6.77 – 6.80]
Biphasic I	$\beta_0 = -2.521_{(.005)}$ $\beta_1 = 0.7826_{(.001)}$	[3.21 – 3.23]	[6.02 – 6.04]
Biphasic II	$\beta_0 = -2.383_{(.005)}$ $\beta_1 = 0.7844_{(.001)}$	[3.03 – 3.05]	[5.83 – 5.85]

$$E = 1 \text{ V/cm}$$

Column 1: DB

Column 2: An

Column 3: De



Background

Model

Equations &
Parameters

Analysis

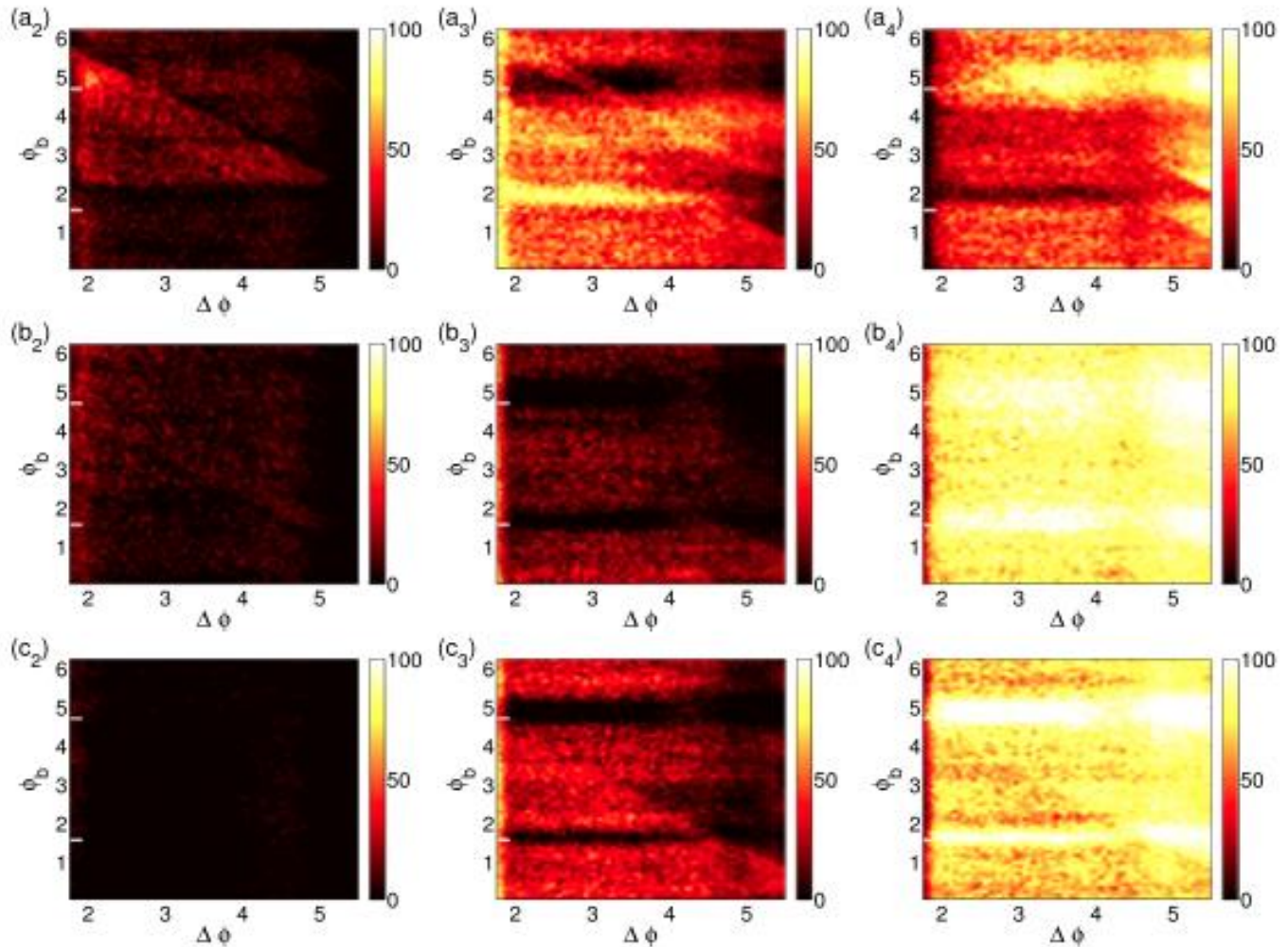
Conclusion

$$E = 7 \text{ V/cm}$$

Column 1: An

Column 2: De

Column 3: DA



Background

Model

Equations &
Parameters

Analysis

Conclusion

Protocol efficiency varies with shock energy

E (V/cm)	Monophasic	Symmetric Biphasic	Asymmetric Biphasic
1	27.50	17.33	15.50
2	34.48	33.10	40.65
3	43.93	43.38	45.13
4	59.93	56.93	60.78
5	75.10	74.75	80.35
6	85.23	90.43	92.13
7	92.50	98.53	97.88
8	96.58	99.90	99.78
9	98.75	100	100
10	99.68	100	100

Background

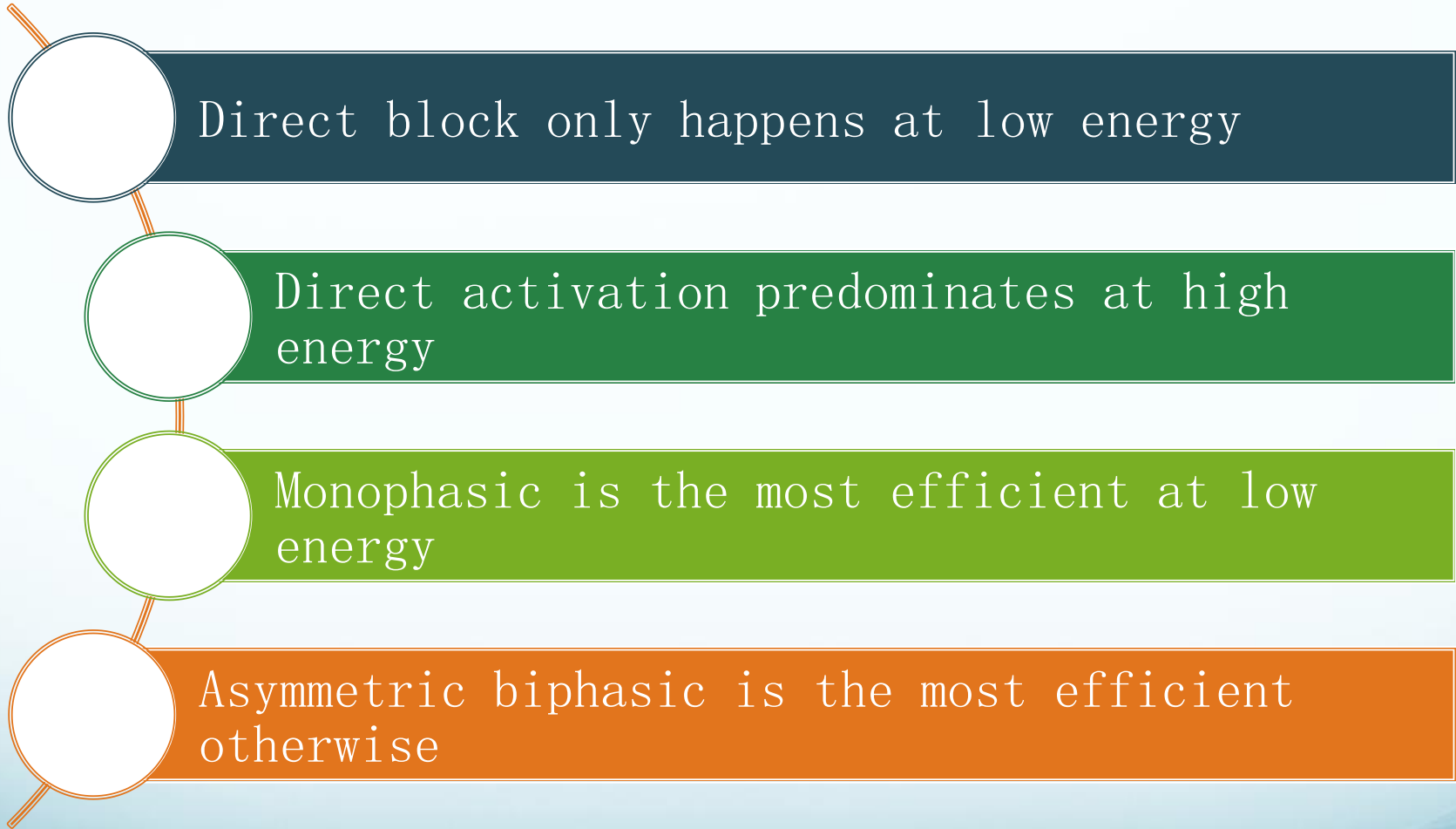
Model

Equations &
Parameters

Analysis

Conclusion

Conclusion



Background

Model

Equations &
Parameters

Analysis

Conclusion

Conclusion

High E \rightarrow 90% success

- The analysis of the numerical data shows that when the energy is high (which E is 7V/cm here) all of these three protocols will achieve 90% success

Efficiency

$Efficiency_{(biphasic_II)} > Efficiency_{(biphasic_I)} > Efficiency_{(monophasic)}$

Future Research

Asymmetric Biphasic

- Shorter first-phase vs. Shorter second-phase

Shock Duration

- Change the shock duration to less than 8 ms

Questions



Background

Model

Equations and
parameters

Analysis

Conclusion
and Next Step